



Basic introduction to multivariate neuroimaging analysis – for nerds and novices

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Buddhist mantra of
cognitive neuroscience:

**“There is no I in fMRI (or
PET)”**

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Opinionated intro

- Not too long ago, a strange “culture war” was going on with multivariate analysis pitted against univariate analysis, at least in fMRI analytics
 - Univariate proponents would claim that multivariate analysis had no false-positive controls
 - Replication and permutation tests were not highly prized
 - Multivariate results were seen as hard to interpret
 - A Yale Biomed-Engineering professor expressed incredulity to me on hearing a talk of mine in 2008: “Multivariate vs. univariate dichotomy is like a war of apples against oranges” – his apt commentary
 - At the same, multivariate analysis had been performed in resting FDG-PET already since 1984 (Horwitz, Rappoport, Moeller, Strother, McIntosh, Eidelberg and many more)
 - **Opinionated take: Today, multivariate analysis and highly derivative frameworks have become very common, sometimes apparently more for intellectual ownership than scientific illumination**
- Molecular connectivity strives for informed use of connectivity approaches, following the tradition of the successful work in PET, while avoiding anti-Occam’s razor tendencies**

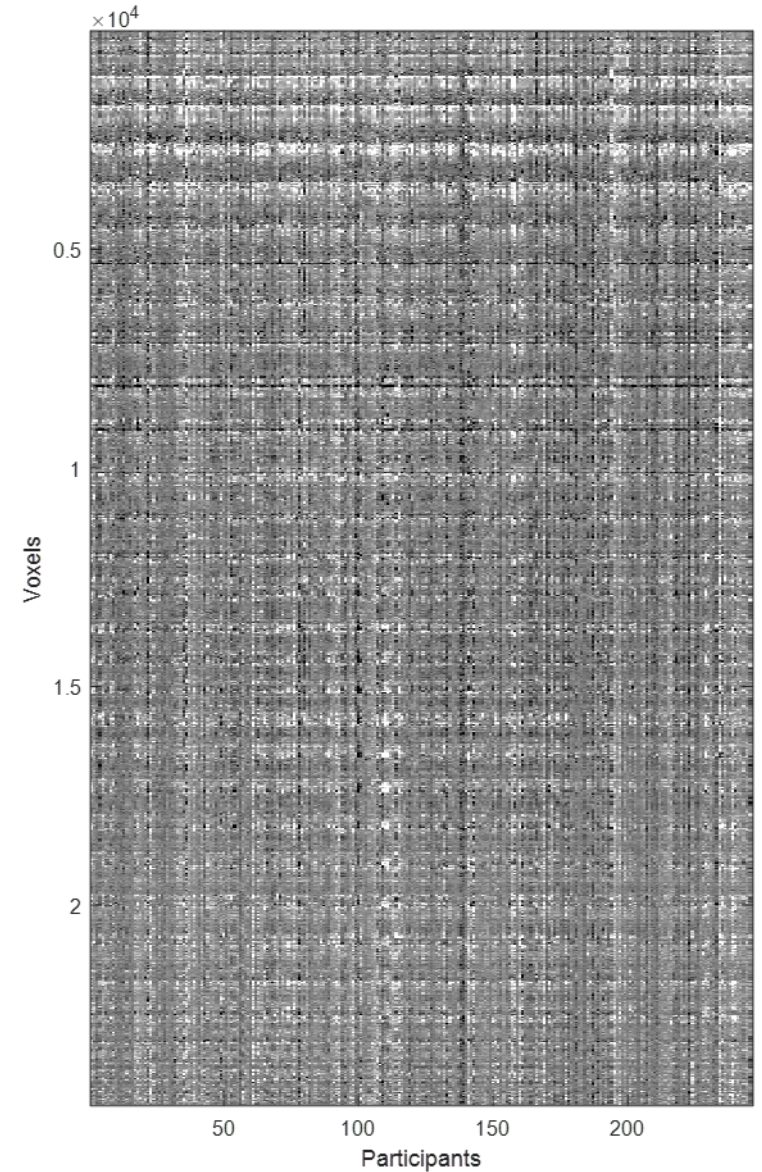
Cross-sectional sample data Y

[Y] = number of voxels x number of participants

V

x

N



Typical univariate analysis

[Y]= number of voxels X number of participants

Perform linear models to assess the influence of covariates in voxel activation

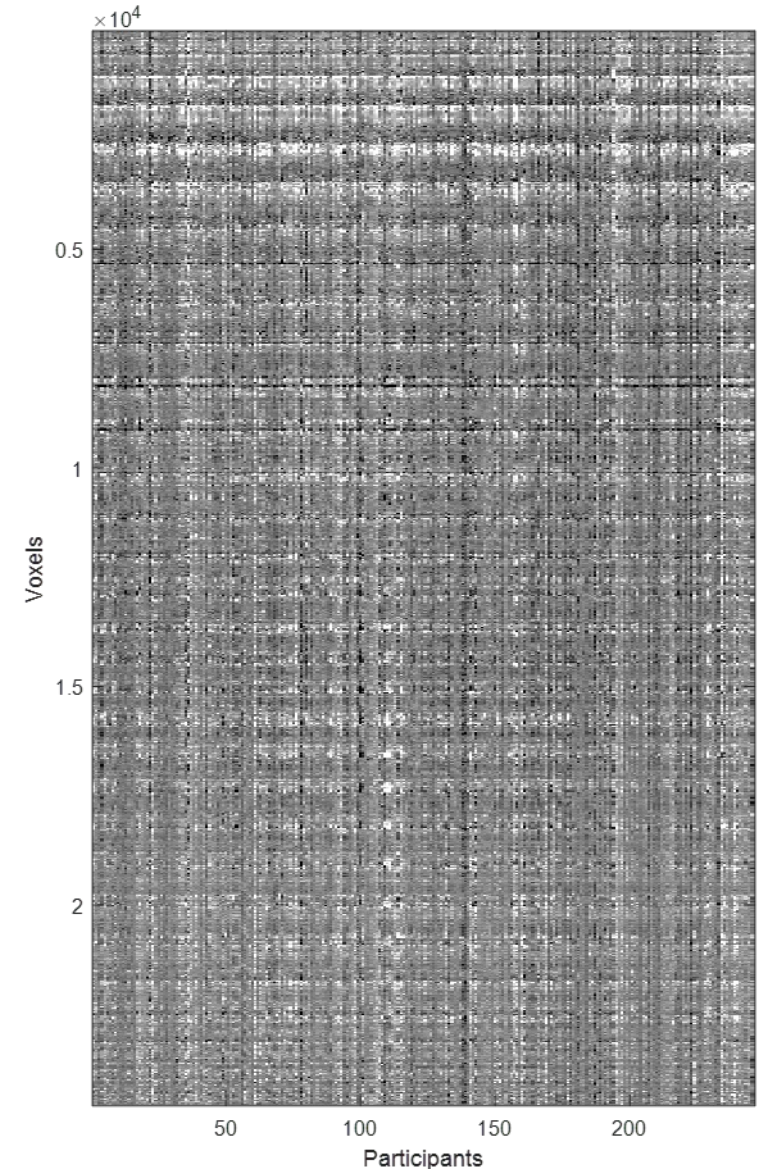
- Linear regression is run within voxel (=row wise), across participants

$$\mathbf{Y}(i) = \mathbf{X} \boldsymbol{\beta}(i) + \boldsymbol{\varepsilon}$$

$i=1\dots V$ voxel location

\mathbf{X} = 'Design matrix'

$\boldsymbol{\beta}$ = parametric maps, dependent on voxel location



Simple dimensional thoughts

[Y]= number of voxels X number of participants

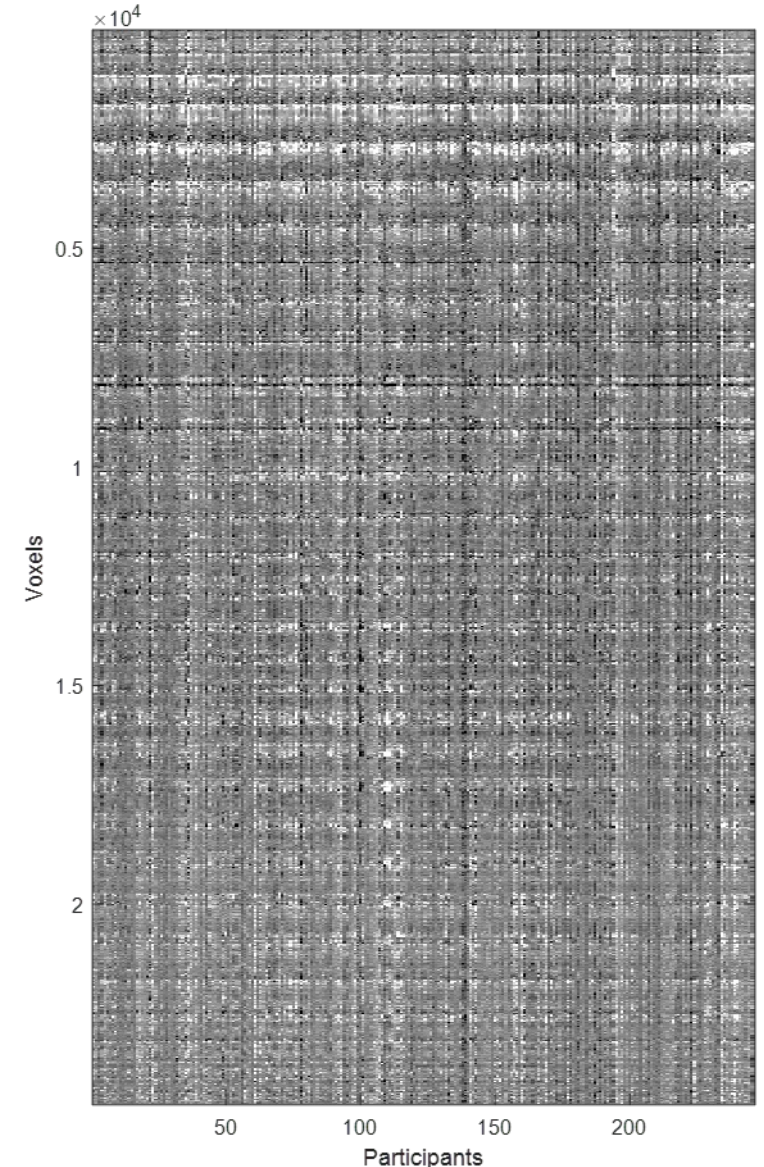
[Y]= number of voxels x number of participants

V x N

Neuroimaging, like genetics, and other fields with increasing data richness often has (several orders) more variables than observations

$$V > N$$

- **Rank (Y) = N** this implies that the maximum number of independent sources in the data is N
- There **must** be correlation between the voxels **by necessity**, prediction of an outcome with $F : R^V \rightarrow \text{outcome}$ has to consider this redundancy



Multivariate analysis

[Y]= number of voxels X number of participants

Multivariate Decompositions - generic form from matrix form of OLS:

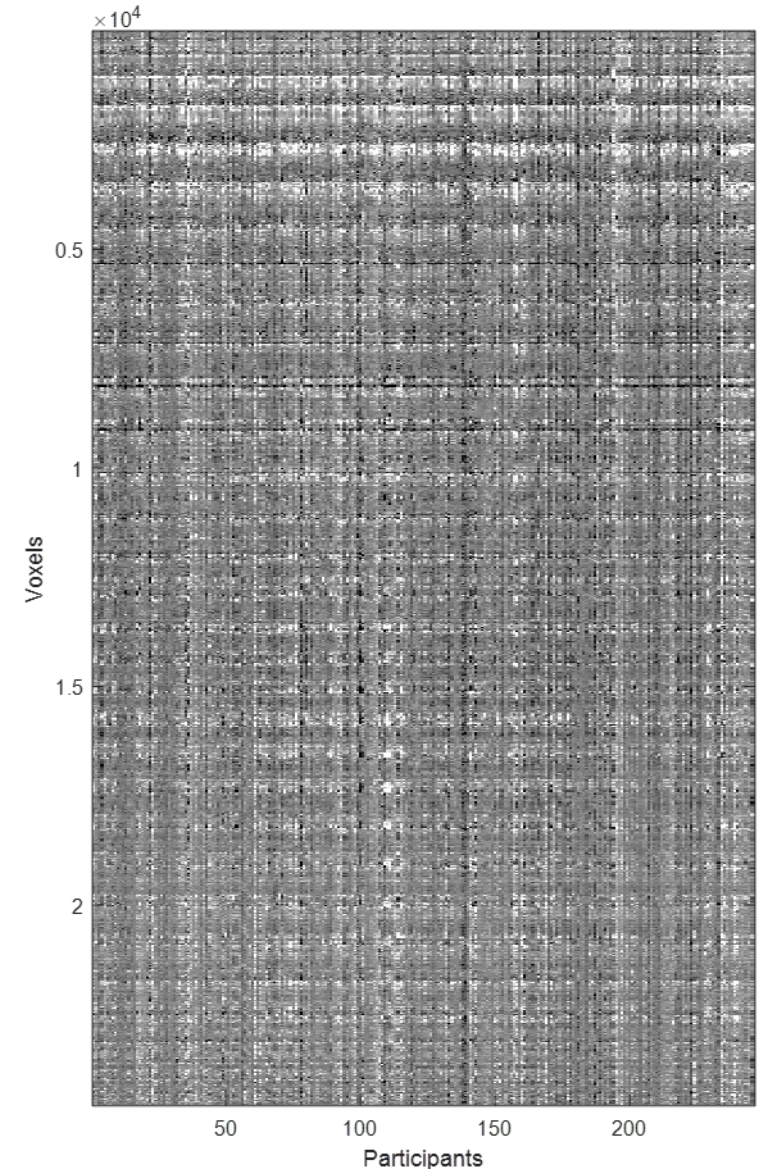
$$Y = V W' + \epsilon$$

V = 'component matrix', columns are components

[**V**] = number of voxels x number of components

W = 'score matrix' or 'mixing matrix', columns are subject expression vectors

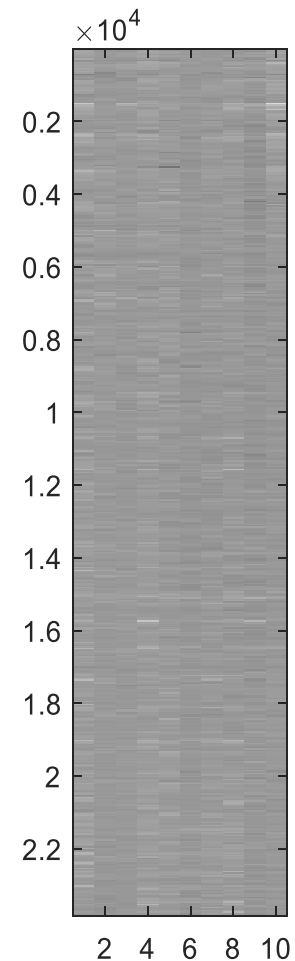
[**W**] = number of subjects x number of components



Generic form of multivariate analysis

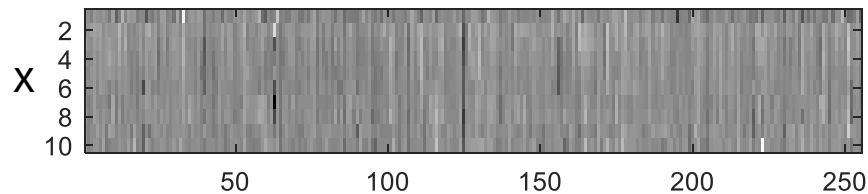
$$Y = V W' + \epsilon$$

[V]=voxels x 10



Assume 10 components, C=10

$W' = 10 \times N$



Possible choices

- **Principal Components Analysis (PCA):** Columns of **V** and **W** are mutually orthogonal
- (Spatial) Independent Components Analysis (ICA): Columns of **V** are mutually statistically independent to all orders
- Non-Negative Matrix factorization (NNMF): **V, W** > 0
- Many more: sparsity of loadings, VariMax, ProMax, etc.
- ***Make your own?***

Don't confuse mathematical convenience of decomposition principles (=sparsity, orthogonality, independence) with scientific meaning!

➔ Need outside validation

PCA didactics - Principal Component Analysis (Karl Pearson 1901)

“Eigen equation” – what is that?

$$\text{COV } \mathbf{v}(i) = \mathbf{Y} \mathbf{Y}' \quad \mathbf{v}(i) = \lambda(i) \mathbf{v}(i)$$

Eigen vectors just get scaled when multiplied by covariance matrix

$$\mathbf{Y} \mathbf{Y}' \mathbf{V} = \mathbf{V} \mathbf{\Lambda} \quad \text{Eigen equation in voxel x voxel space}$$

$$\mathbf{Y}' \mathbf{Y} \mathbf{Y}' \mathbf{V} = \underbrace{\mathbf{Y}' \mathbf{V}}_{\mathbf{W}} \mathbf{\Lambda} \quad \implies \quad \mathbf{Y}' \mathbf{Y} \mathbf{W} = \mathbf{W} \mathbf{\Lambda} \quad \text{Eigen equation in subject x subject space}$$

\mathbf{W} = subject eigen vectors

\mathbf{V} = voxel eigen vectors = brain images

$\mathbf{\Lambda}$ = diagonal Eigen value matrix

$\mathbf{Y} = \mathbf{V} \text{sqrt}(\mathbf{\Lambda}) \mathbf{W}'$ (=SVD)
“singular value decomposition”

PCA didactics

$$Y = V(:,1) \lambda(1) W(:,1)' + V(:,2) \lambda(2) W(:,2)' + V(:,3) \lambda(3) W(:,3)' + \dots$$

$$Y = V \text{sqrt}(\Lambda) W' \quad (=SVD)$$

“singular value decomposition”

$$\text{with } W \rightarrow W \text{sqrt}(\Lambda): \quad Y = V W'$$



Decomposition into orthogonal components in descending variance order without inherent stochastic variability

Objective: truncate at the right place to capture signal, and split off noise

$$Y = V(:,1:C) W(:,1:C)' + \epsilon \quad \text{for } C \text{ components}$$

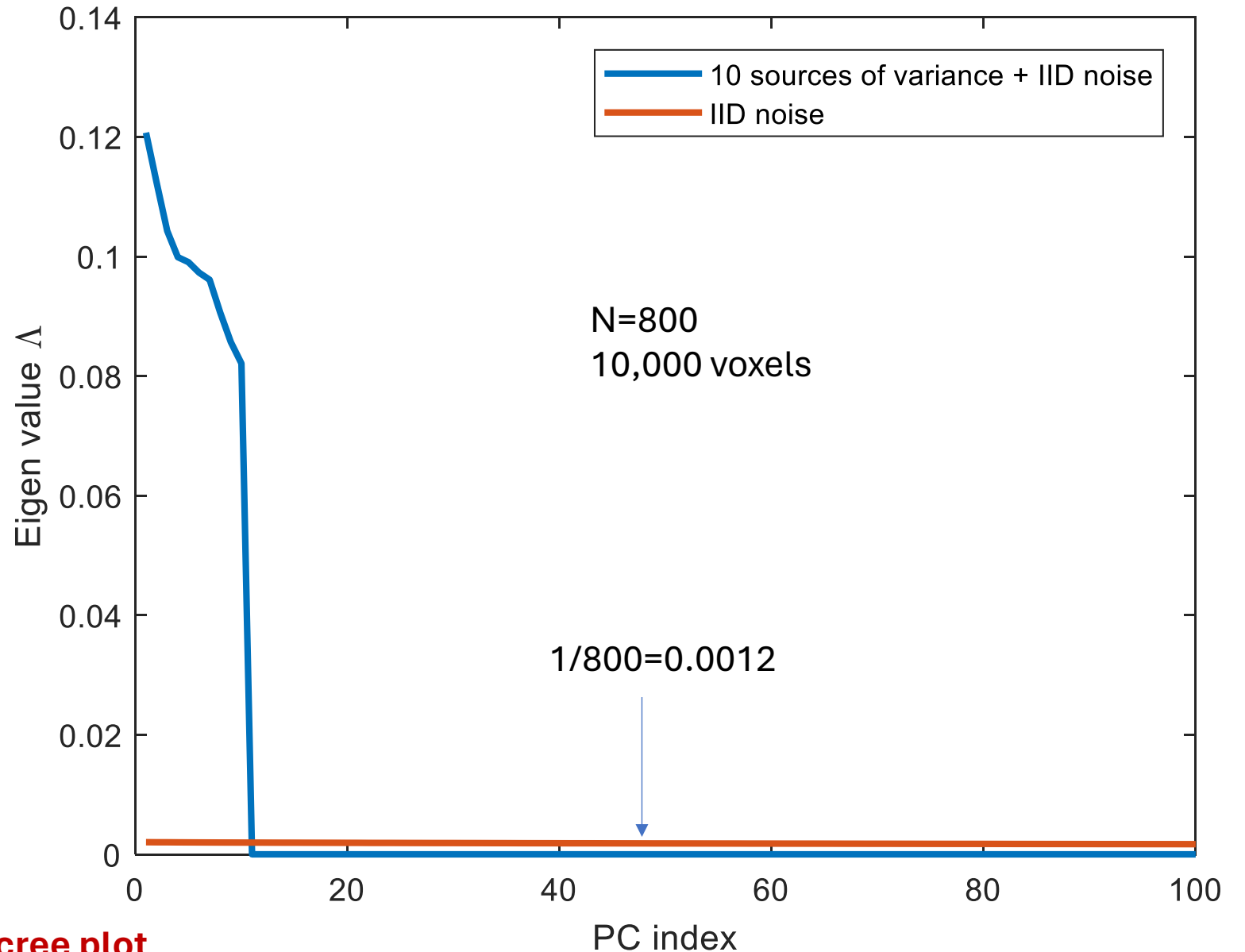
Scree plot for PCA: compute Eigen values λ (=VAF) from whole PC- spectrum

PCA (Y) \rightarrow (W,V, Λ)

\rightarrow Normalize that λ s sum to 1

\rightarrow The flatter the scree plot, the more independent sources in the data

\rightarrow Pure voxel noise gives approximate $1/N$ line

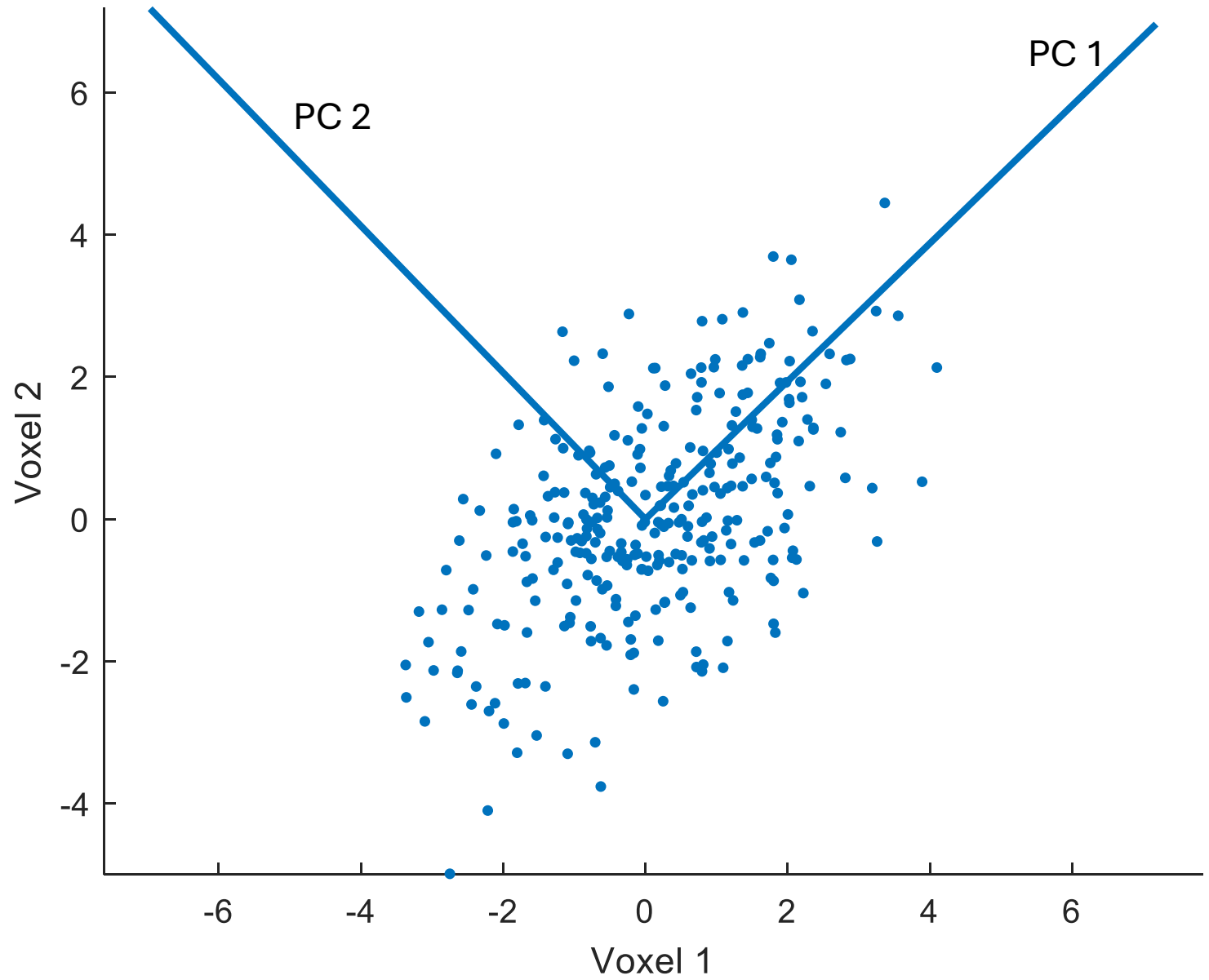


Simplest visual heuristic: “kink” in scree plot
Others: AIC, BIC, MDL, CP-Mallows, N-fold-CV

PCA didactics II

Toy data sets with only 2 voxels

V =
0.7178 0.6962
0.6962 -0.7178



PCA didactics III

What happens with prior data reduction?

MLM, CCA, PLS, etc. ...

Data get reduced with pre-transformation

V-FULL =

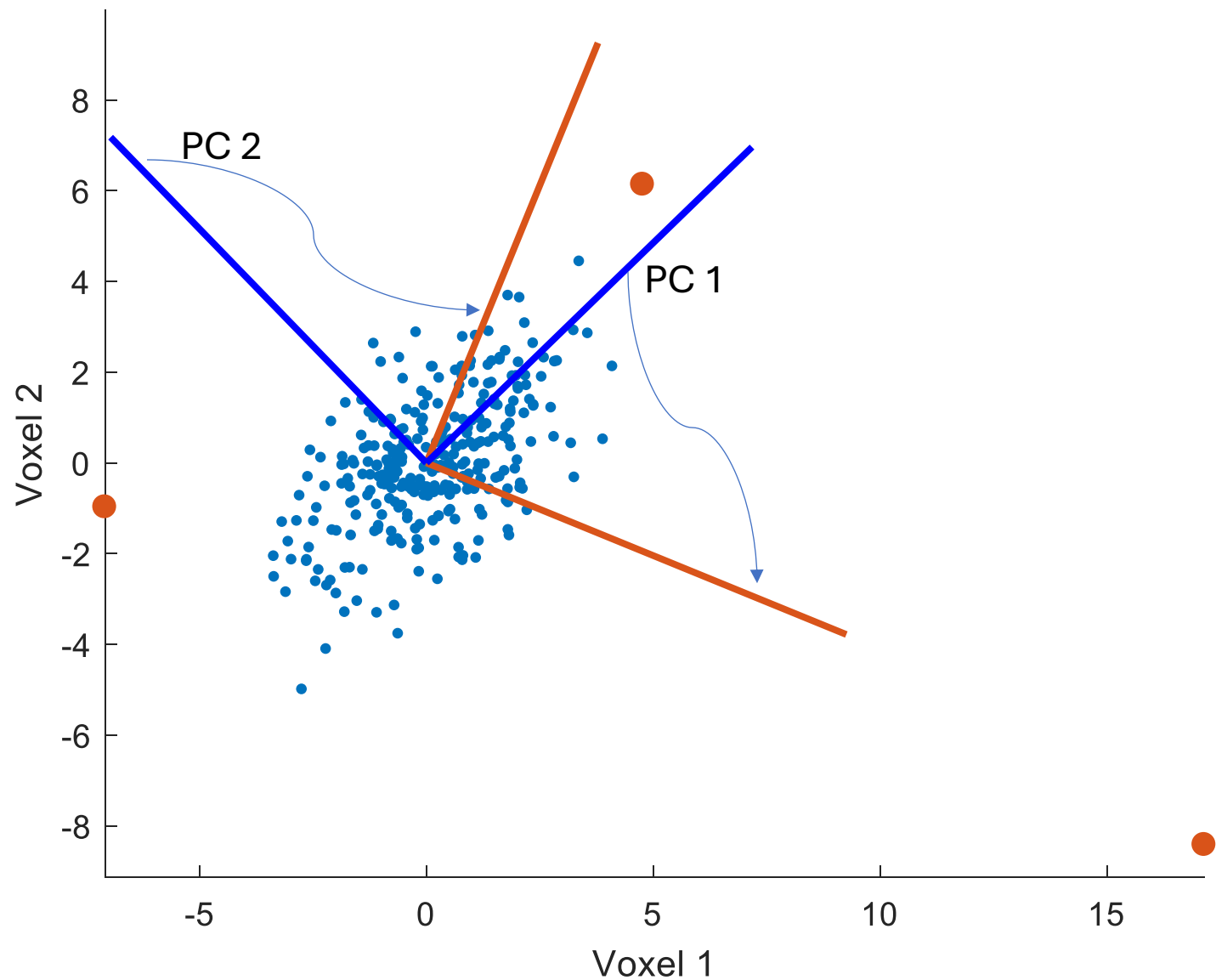
0.7178 0.6962

0.6962 -0.7178

V-REDUCED =

0.9257 0.3782

-0.3782 0.9257



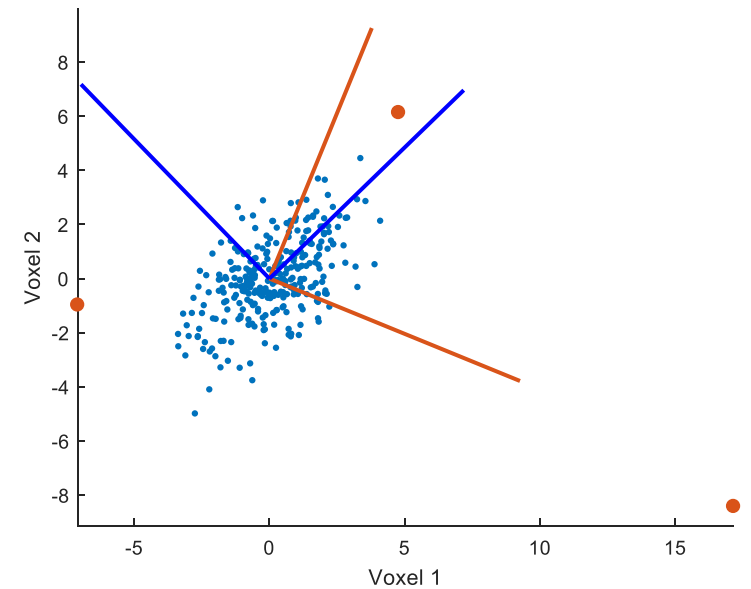
PCA didactics III

What happens with prior data reduction?
MLM, CCA, PLS, etc. ...

Data get reduced with pre-transformation

$$V\text{-FULL} = \begin{pmatrix} 0.7178 & 0.6962 \\ 0.6962 & -0.7178 \end{pmatrix}$$

$$V\text{-REDUCED} = \begin{pmatrix} 0.9257 & 0.3782 \\ -0.3782 & 0.9257 \end{pmatrix}$$



Christian's opinion:

Don't reduce data prior to PCA with CCA or PLS, the results appear less arbitrary and more rigorous, and seemingly forgo the need for subset selection - but you are potentially throwing out baby with the bath water and might lose important signal!

(Cf. Simpson's paradox)

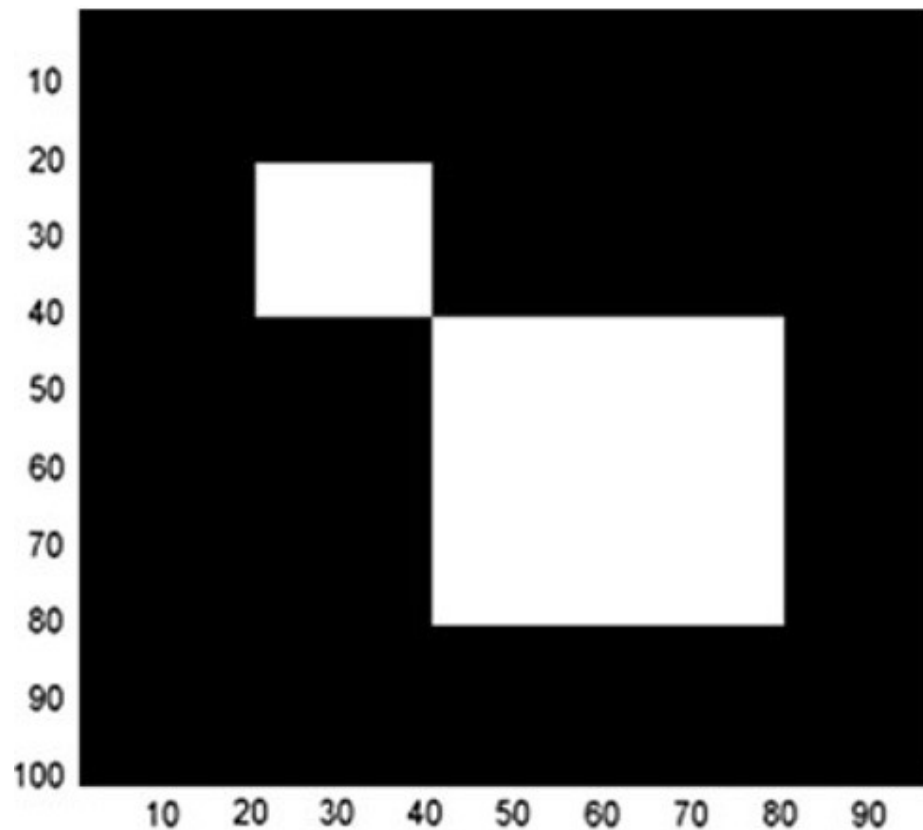
Brief excursion to didactic article with 2-d example

[Cell Biochem Biophys.](#) 2010 Nov;58(2):53-67. doi: 10.1007/s12013-010-9093-0.

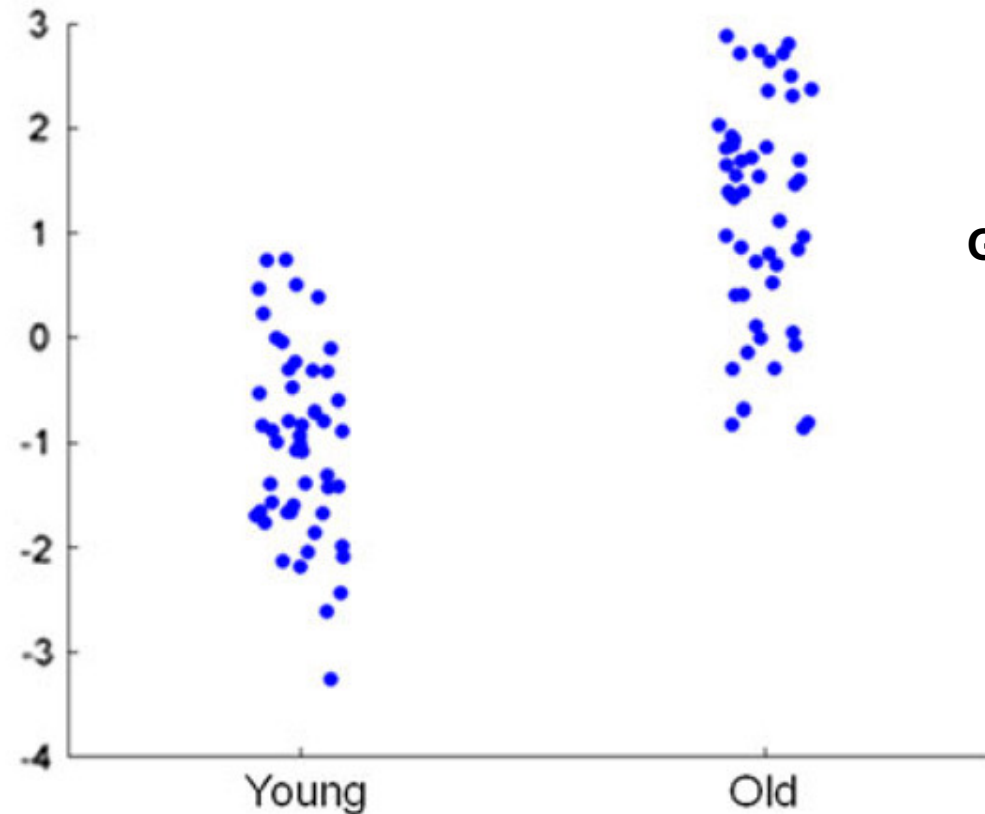
Multivariate data analysis for neuroimaging data: overview and application to Alzheimer's disease.

[Habeck C¹](#), [Stern Y](#); [Alzheimer's Disease Neuroimaging Initiative](#).

$$Y = v w' + \epsilon$$



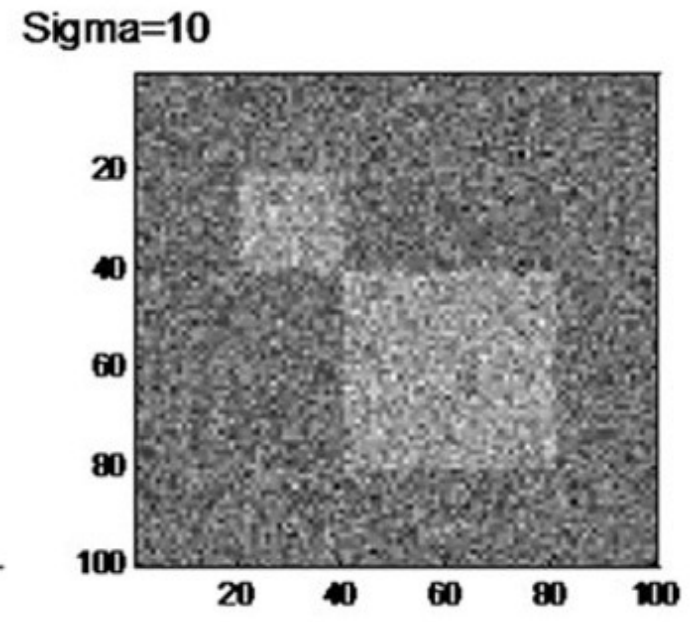
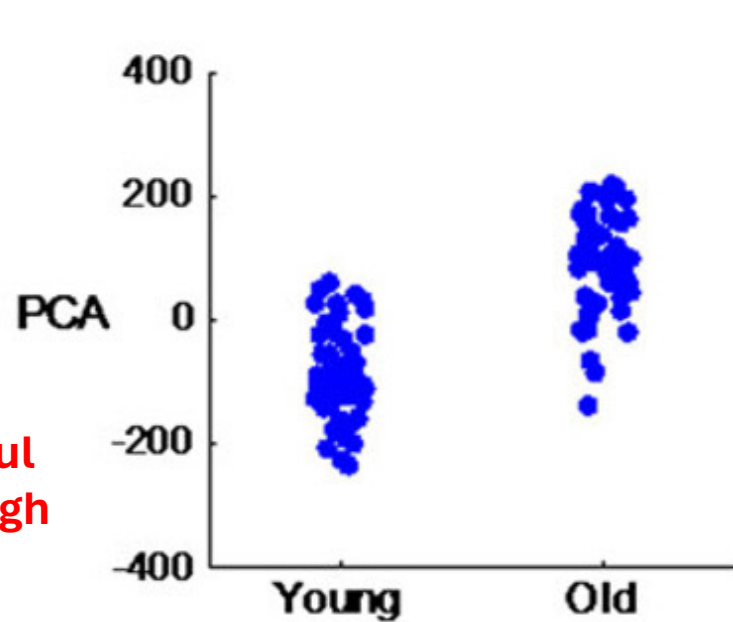
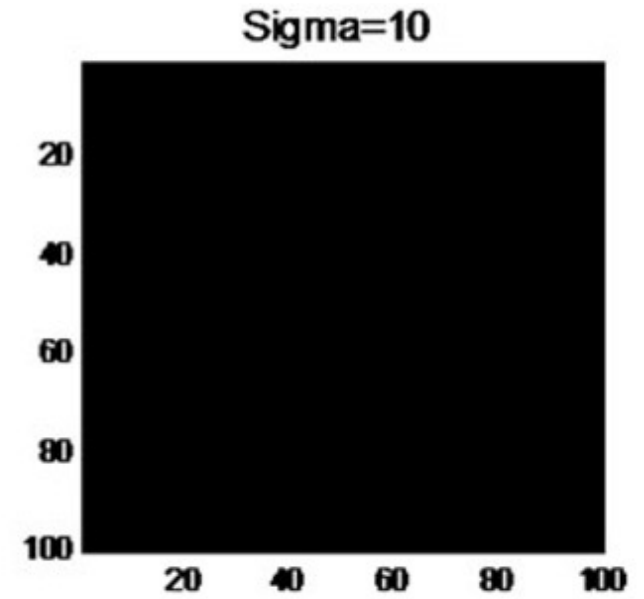
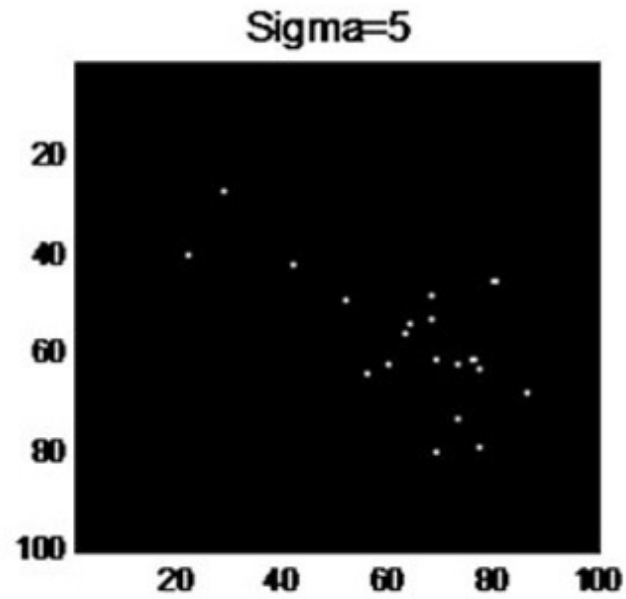
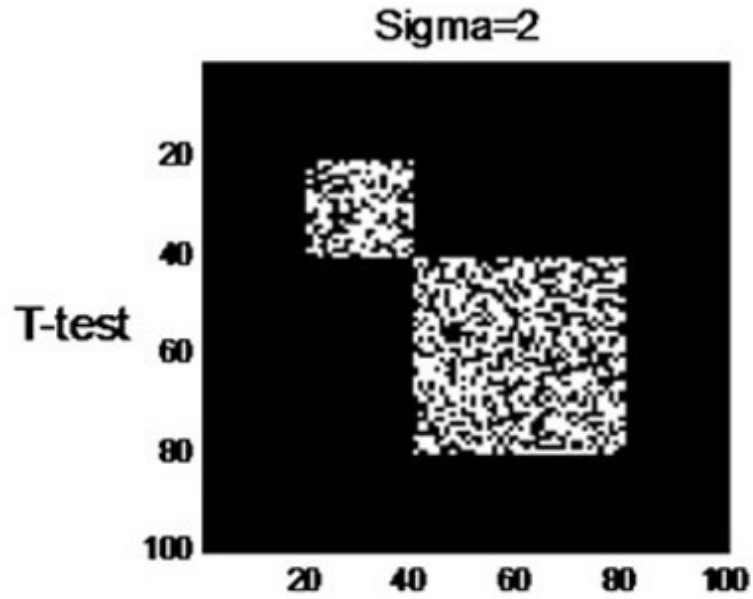
v = pattern



w = subject score vector

Gaussian pixel noise:
 $\epsilon \sim N(0, \sigma^2)$

Different noise levels



→ Multivariate analysis is more powerful
→ Distributed nature of activation though is key

Out-of-sample validation via prospective application



Nice feature of multivariate patterns: **the pattern can be prospectively applied to any data set to yield a pattern score**, and verify correlations between the pattern score and a cognitive or clinical endpoint **even if the pattern was generated from a different data set**

$$\text{score} = \text{DATA}' * \text{pattern}$$

$$[\text{score}] = N \times 1$$

$$[\text{DATA}] = \text{voxels} \times N$$

$$[\text{pattern}] = \text{voxels} \times 1$$

→ Both pattern and DATA need to be resliced into the same voxel space, obviously

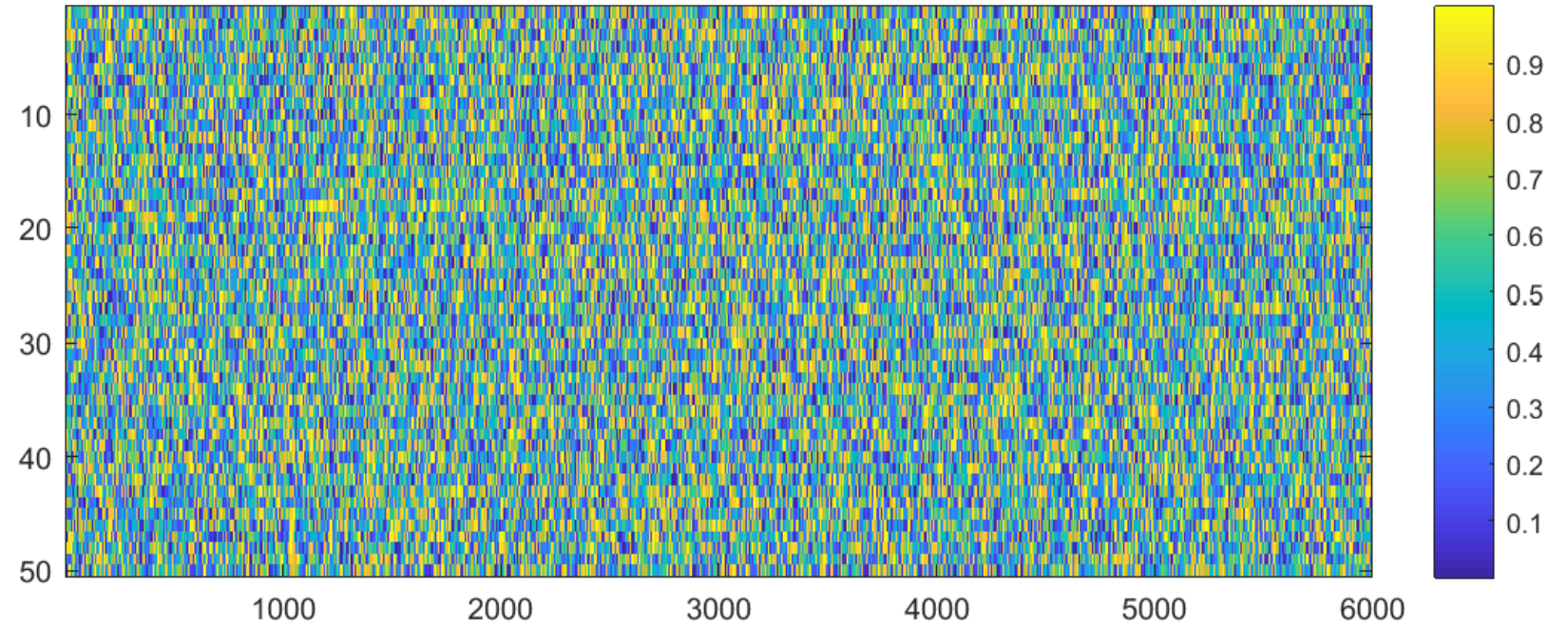
Recent “caveats” about PCA

Some caveats about PCAs have been highlighted recently and mainly address well-documented overreach in the interpretation

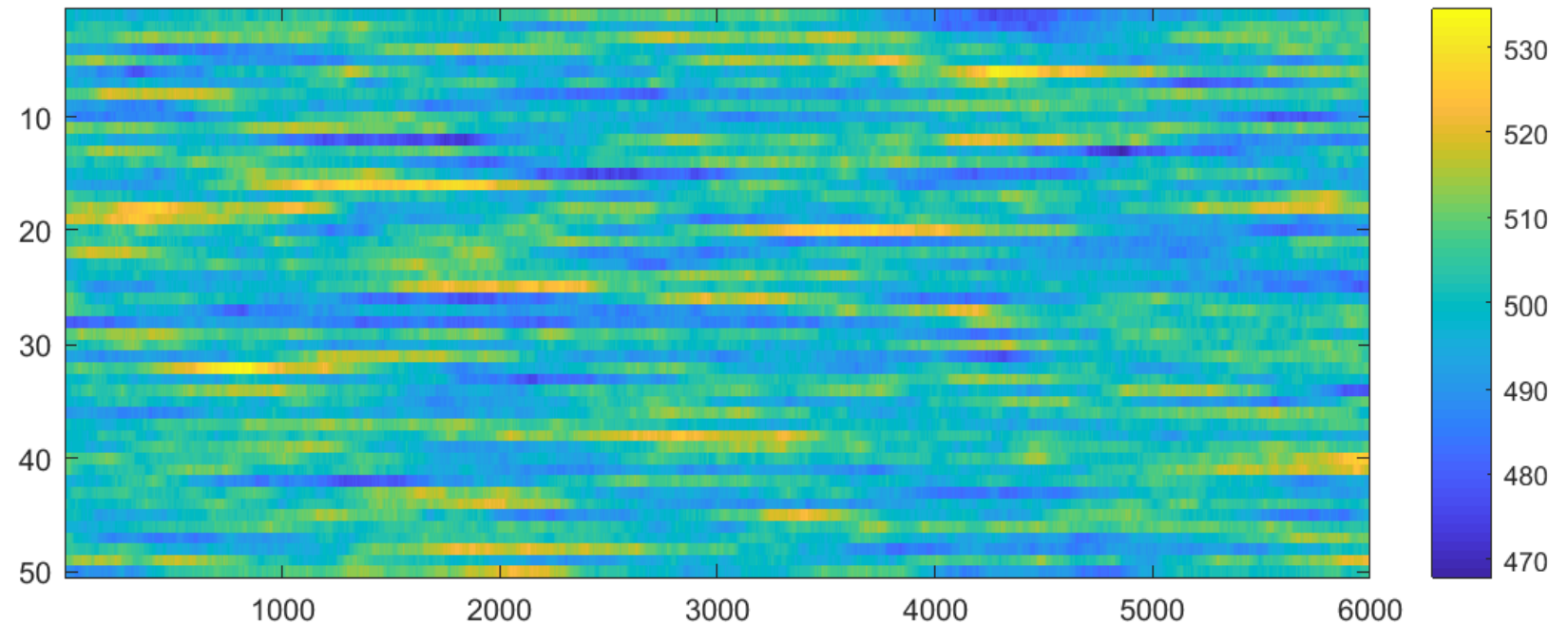
- PCA (or other multivariate decompositions like ICA, NMF, clustering) produce components regardless of neurobiological meaning – without outside information for validation, i.e., association with a meaningful endpoint, the evidence is much weaker
- Picking single principal components, particularly with small variance contribution, is problematic because of sampling variability and noise

“One man's trash is
another man's treasure”
- PCA works on every
kind of signal

50 temporal null
signals without
correlation

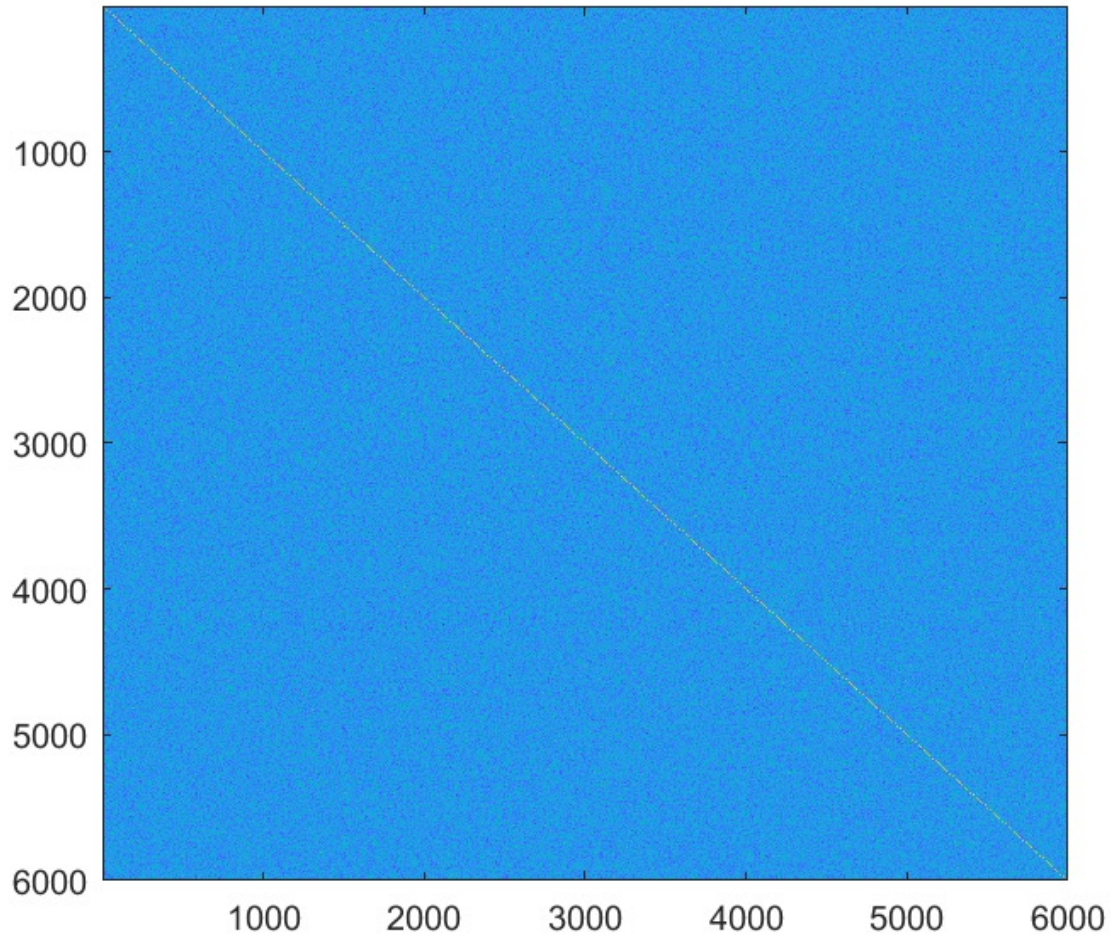


50 null signals
after smoothing
with a 1000-step
moving window
average

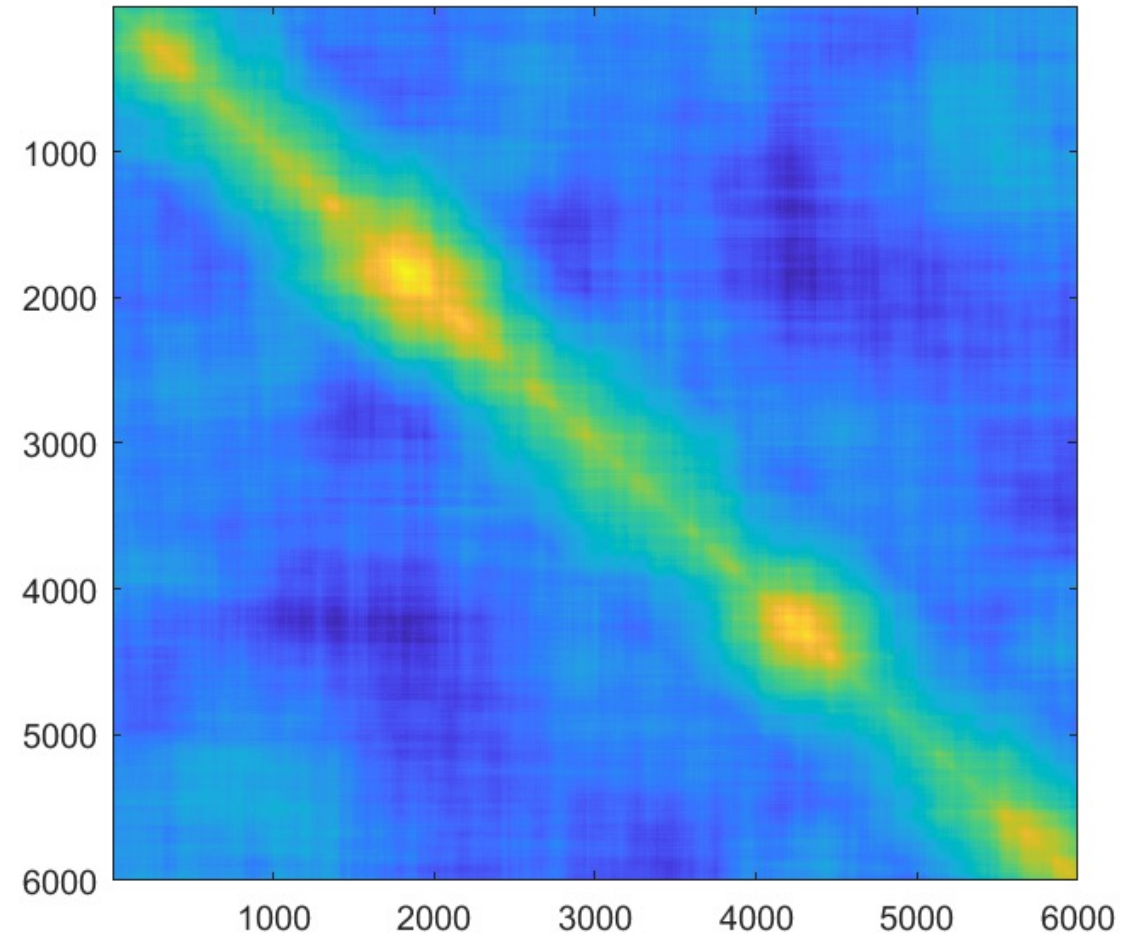


Computing time-domain covariance matrix

Covariance unsmoothed

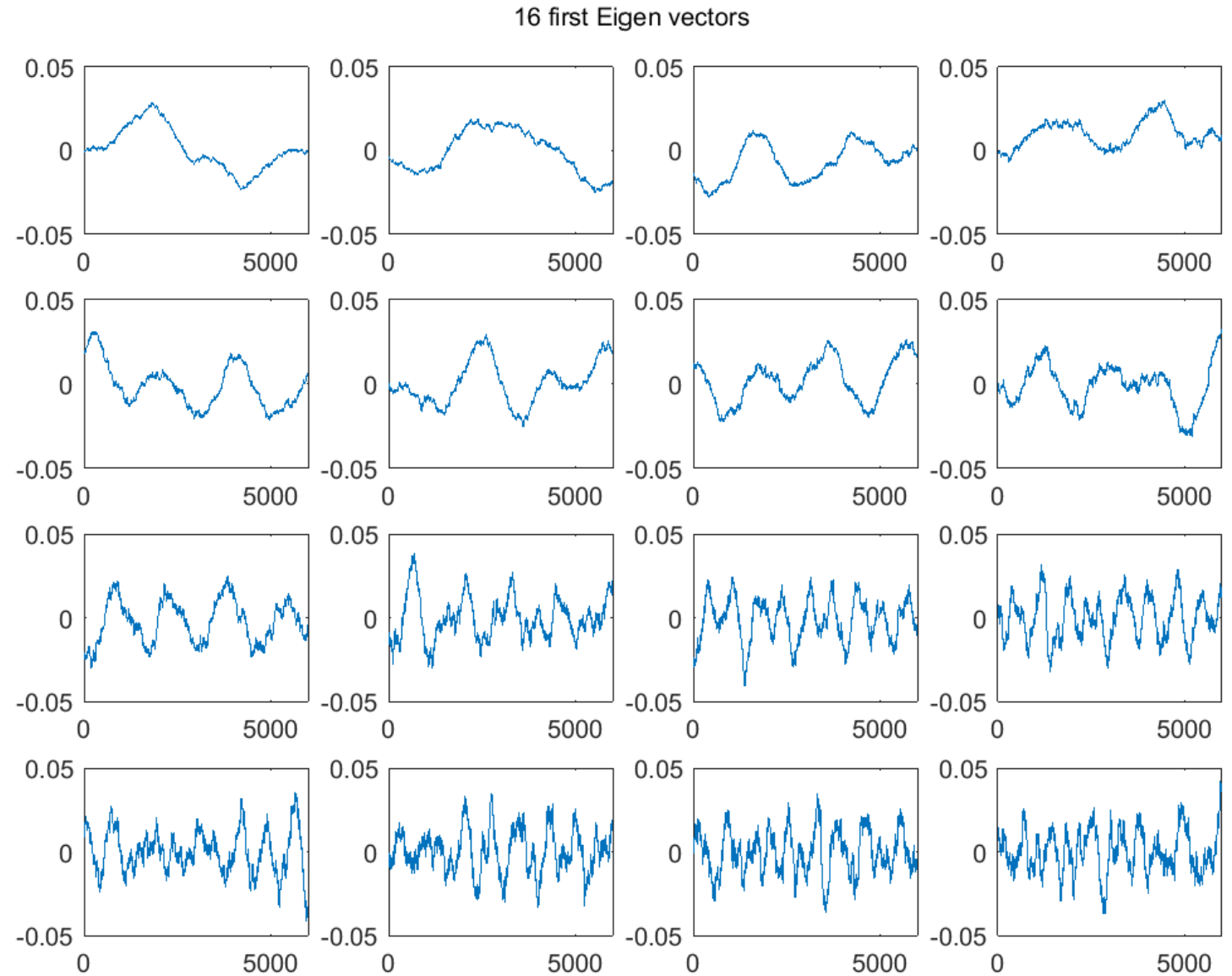


Covariance smoothed



Eigen vectors show harmonics, despite any meaningful correlation structure in null signals

Picking one isolated component would yield meaningless sinusoidal signal

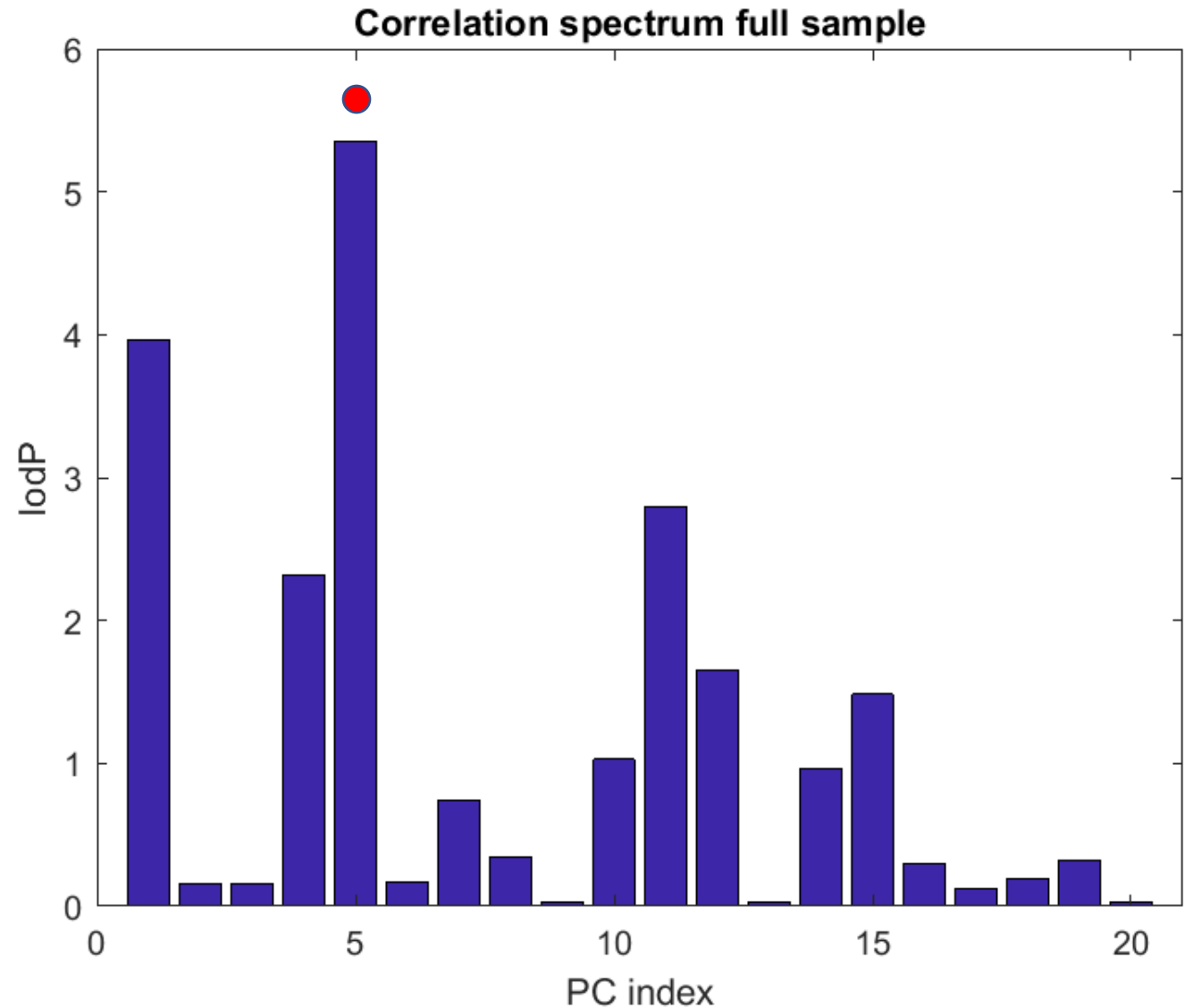


→ Simple safeguard: replication out of sample, including components loadings AND prediction of an endpoint!

Real-world example in a Fluid Reasoning task (“Paper Folding”) in 324 people aged 20-80

- Activation maps from event-related designs
- Recognition accuracy is the behavioral variable

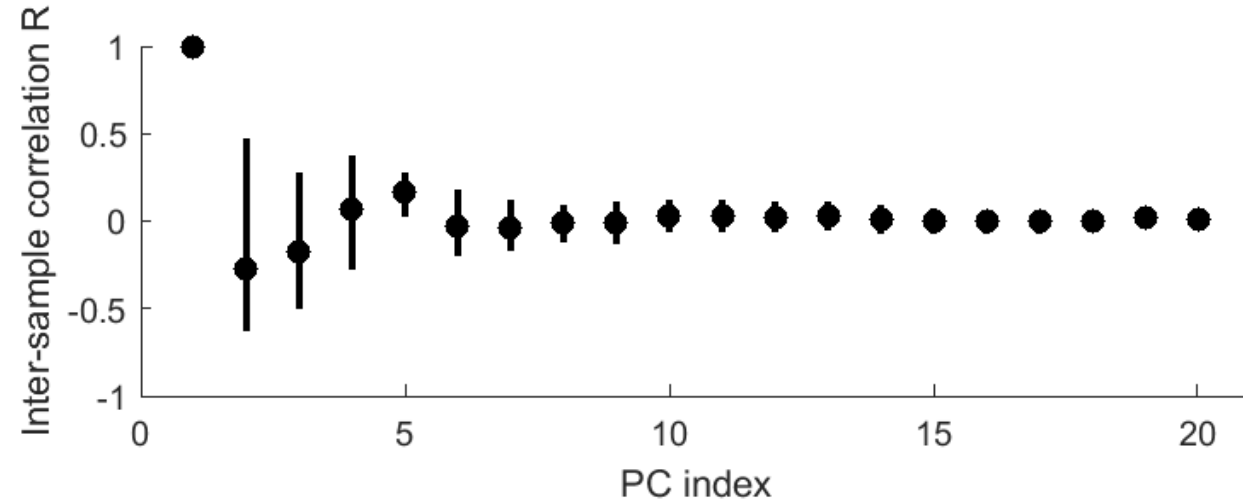
→ Perform PCA and check first 20 PC-scores and their correlation with recognition



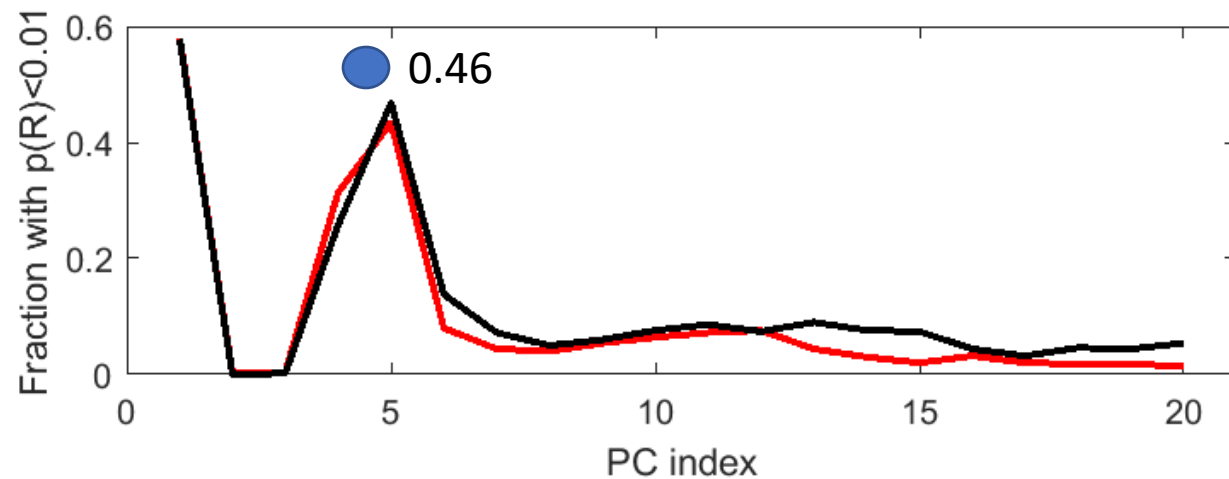
Divide randomly into non-overlapping training and test of 150/150

Test behavioral correlation of subject scores in both samples, subject scores are obtained from PCs from training sample

**Spatial correlation
between two PC-sets
samples**



**Correlation with
behavior in both training
and test samples**



Multivariate Analysis Framework

Multivariate Analysis framework

- Step 1: PCA on fMRI data

$$\mathbf{Y} = \mathbf{V} \mathbf{W}'$$

\mathbf{Y} = fMRI Data, \mathbf{V} = PC components, \mathbf{W} = scores

- Step 2: Brain-behavior modeling

$$\text{Cognition} = [\mathbf{W}(:,1:K) \quad \mathbf{1}] * \boldsymbol{\beta} + \boldsymbol{\varepsilon}$$

K = number of included PCs determined with AIC or LOOCV

- Step 3: Construction of corresponding brain pattern

$$\text{pattern} = \mathbf{V}(1:k) * \boldsymbol{\beta}(1:K)$$

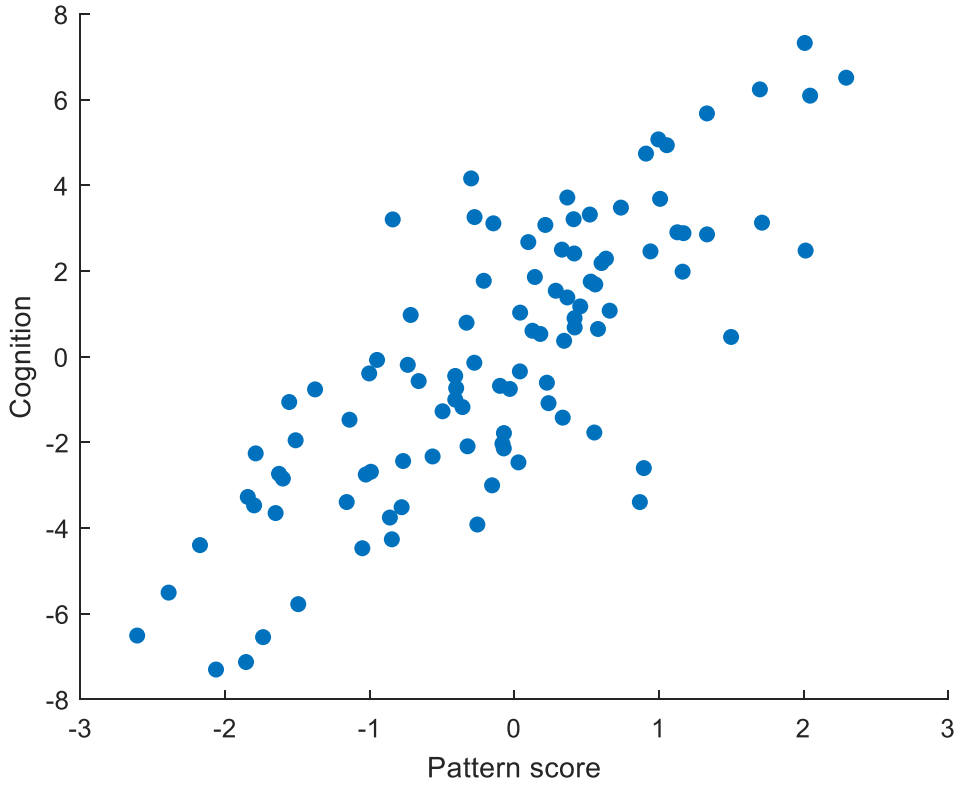
- Step 4: Application of brain behavioral model to held-out data \mathbf{Z} and compute R^2

$$R(\mathbf{Z}' \text{ pattern, cognition in } \mathbf{Z})$$

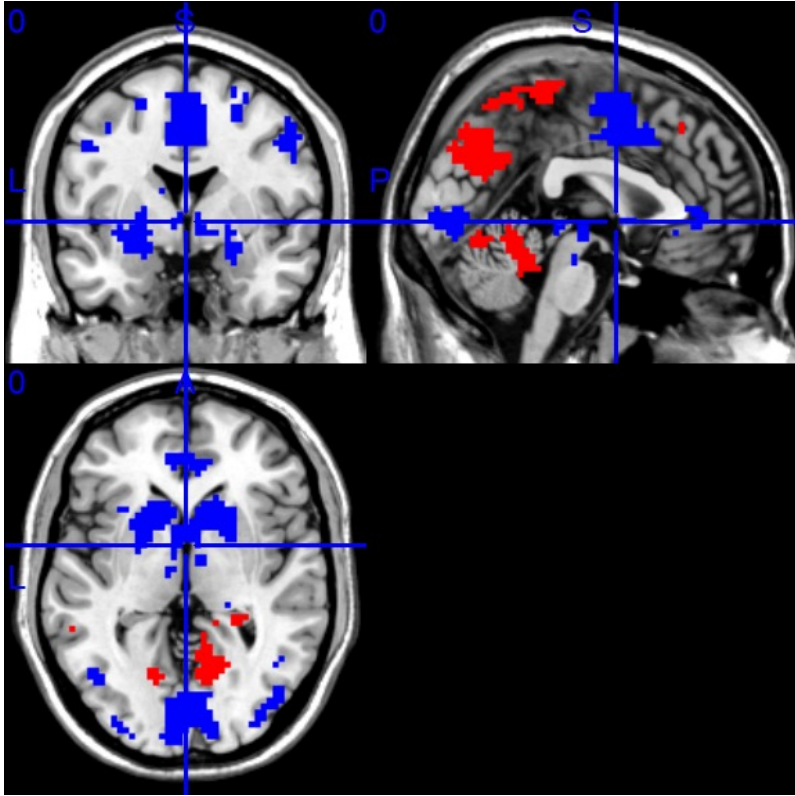
doi: 10.1038/jcbfm.1987.118.
Scaled subprofile model: a statistical approach to the analysis of functional patterns in positron emission tomographic data

[J R Moeller](#)¹, [S C Strother](#), [J J Sidtis](#), [D A Rottenberg](#)

SSM objectives and outcomes



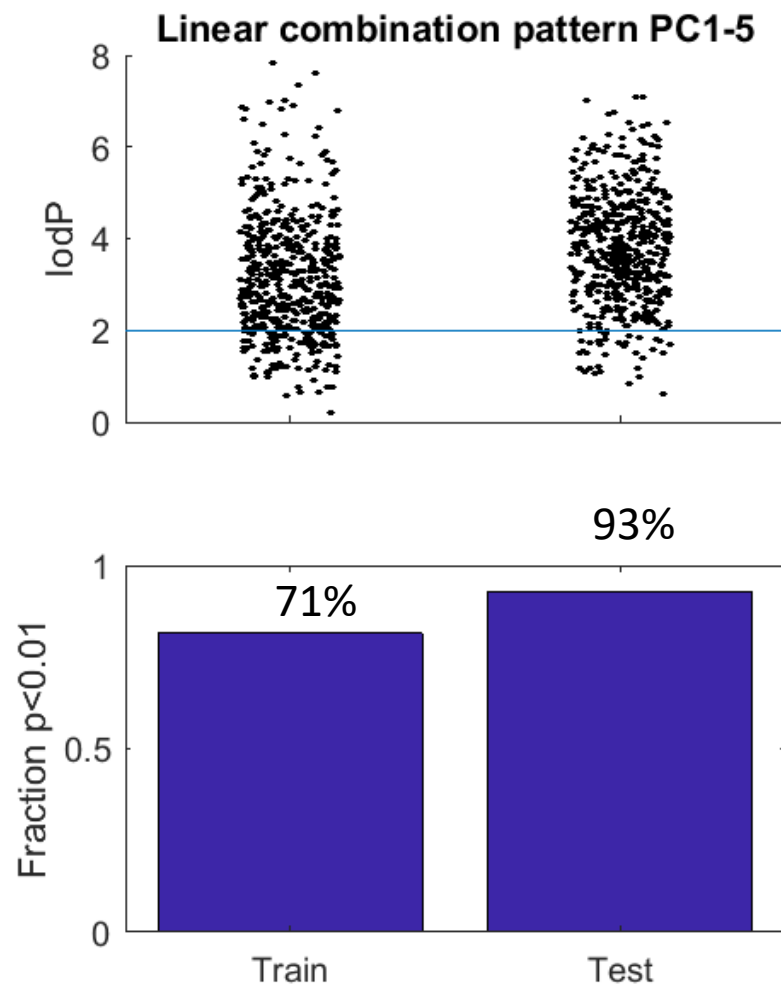
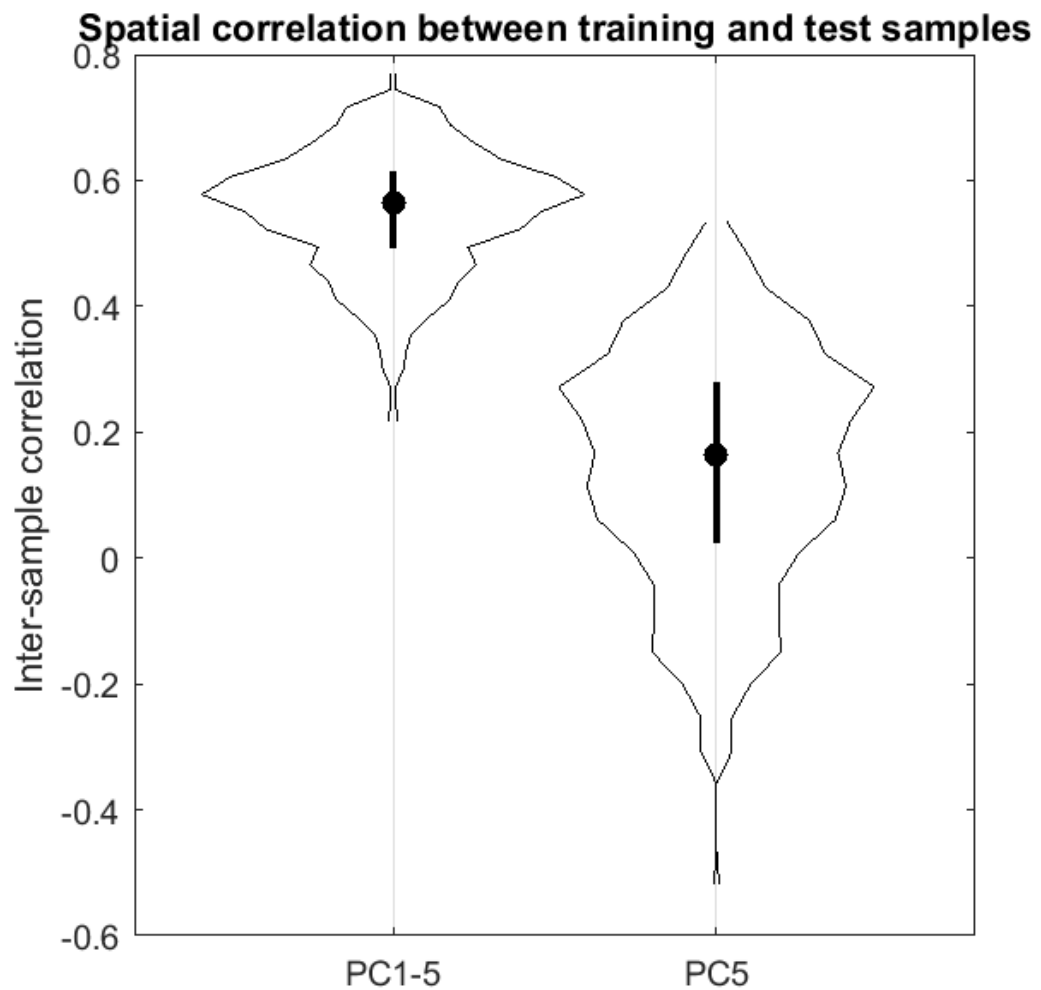
Topographic robustness assessed with bootstrap



$$Y = \text{score} * \text{pattern}' + \epsilon$$

A blue arrow points from the equation to the brain topographic maps.

Use set PC1-5 instead of just PC 5



Replication of performance correlation in test sample: $P(\text{PC1-5}) = 0.93$, $P(\text{PC5}) = 0.46$

Data

fMRI Data Sample

- We use 3 fluid-reasoning tasks which have been acquired in 290 people in the context of the Reference ability neural network study, age 20-80
- The tasks are fMRI recognition versions of:
 - (1) **Matrix Reasoning** (= a visuo-spatial completion task like Raven's Advanced Matrices),
 - (2) **Letter Sets** (= 5 groups of letter sets with identification of one set being the odd one and violating an implicit to-be-discerned rule),
 - (3) **Paper Folding** (= depiction of a paper-folding process with subsequent punching by a stapler and a selection of possible punch-patterns from which the participant chooses)
- The cognitive outcome is the fraction of correct responses

Univariate Analysis Framework

Univariate Analysis framework

- Step 1: Univariate regression

$$\mathbf{y} \sim \mathbf{Y}(:,\mathbf{k}) + \mathbf{1}$$

\mathbf{k} = voxel index

- Step 2: assembly of brain maps $\beta\mathbf{1}(\mathbf{k})$ and $\beta\mathbf{0}(\mathbf{k})$

- Step 3: out-of-sample prediction of cognitive end point for each voxel

$$\mathbf{y}(:,\mathbf{k}) = \mathbf{Y}(:,\mathbf{k}) \beta\mathbf{1}(\mathbf{k}) + \beta\mathbf{0}(\mathbf{k})$$

- Step 4: form a “vote” that weights and averages the voxel prediction in held-out data according to whole-model significance F in training sample

- Step 5: Application of brain behavioral model to held-out data \mathbf{Z} and compute R^2

\mathbf{R} (vote, cognition in \mathbf{Z})

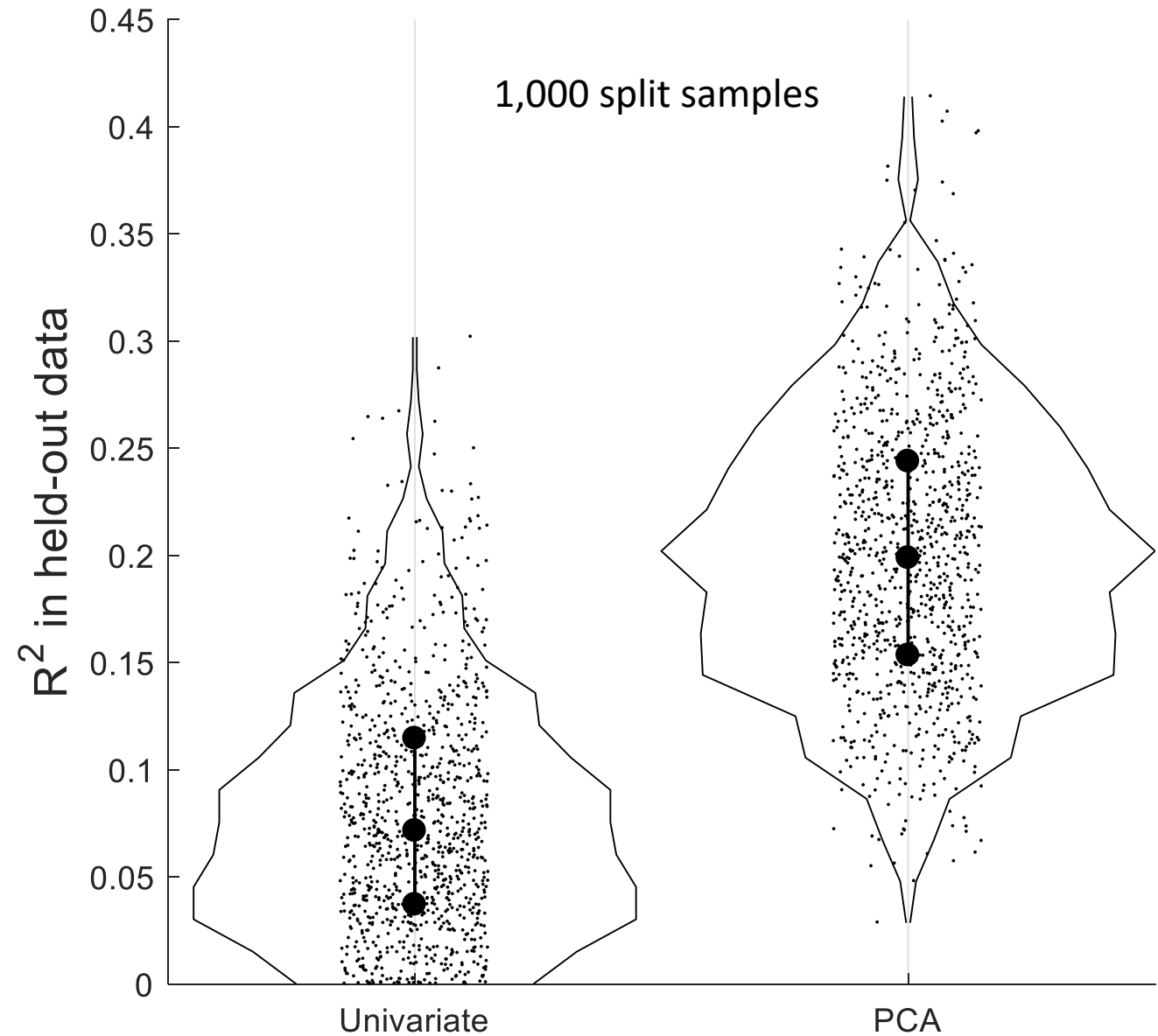
Check in comparison to univariate approach in real-world fMRI data

Training N=600
Test N=100

290 subjects in 3 Fluid Reasoning tasks (=870 observations)

Endpoint: accuracy on recognition task

Compare SSM and univariate approach, with pooling of predictions weighted according to significance in training sample



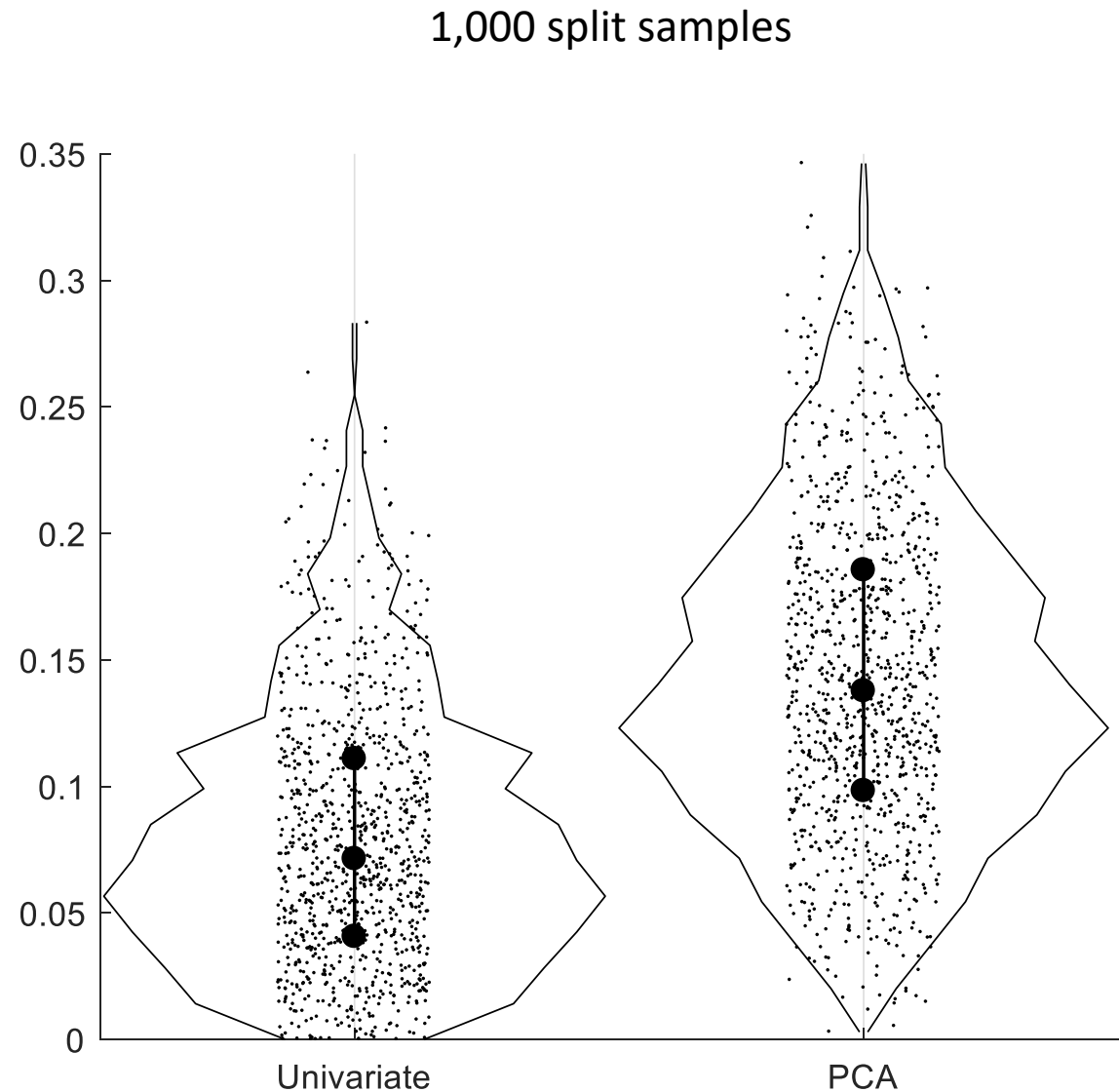
Avoid rank deficiency and pick 500 randomly sampled voxels and repeat

Training N=600
Test N=100

290 subjects in 3 Fluid Reasoning tasks (=870 observations)

Endpoint: accuracy on recognition task

Compare SSM and univariate approach, with pooling of predictions weighted according to significance in training sample



→ PCA loses information, but still beats univariate prediction

Avoid rank deficiency and pick 50 randomly sampled voxels and repeat

Training N=600

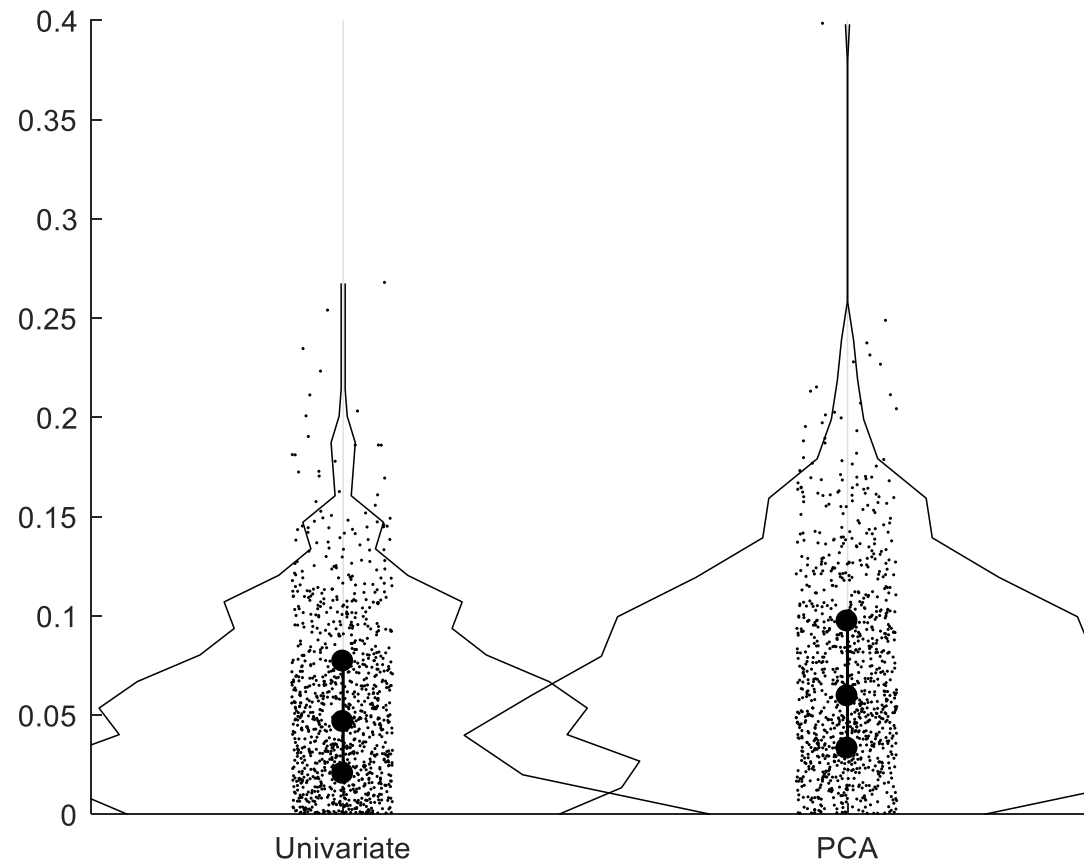
Test N=100

290 subjects in 3 Fluid Reasoning tasks (=870 observations)

Endpoint: accuracy on recognition task

Compare SSM and univariate approach, with pooling of predictions weighted according to significance in training sample

1,000 split samples



→ PCA loses information and approaches univariate performance

Broad takeaway points



- PCA-regression (=SSM) technique achieves better held-out data replication for a Fluid reasoning fMRI task
- This generalizes to other tasks as well (although I did not show the data)
- Reducing the rank deficiency degrades the multivariate predictive utility, whereas the univariate prediction does not suffer; however, multivariate analysis still performs better
- Sampling variability dictates to pick a set of principal components, rather than picking isolated ones
- Rank deficiency necessitates non-parametric statistics, like bootstrap

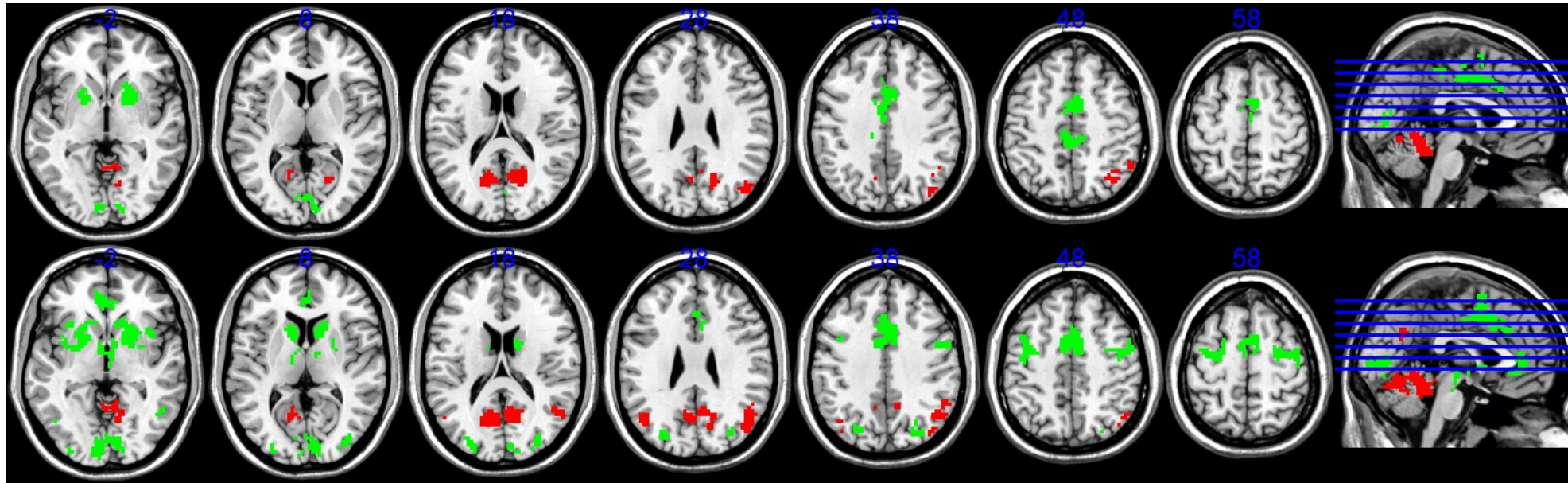
How to generate inferential brain maps when there is no parametric theory? (number of voxels \gg number of observations)

- Point estimate pattern coming from SSM technique

$$\mathbf{v} = \text{SSM}(\mathbf{Y}, \text{Cog}) \quad - \quad \text{pseudo-function notation}$$

- Perform semi-parametric bootstrap, i.e., resample with replacement $\sim 100-1,000$ times
 $\mathbf{v}^* = \text{SSM}(\mathbf{Y}^*, \text{Cog}^*)$ and observe variability about point estimate and generate Z-robustness map

$$Z(\text{voxel}) \sim \text{loading}(\text{voxel}) / \text{STD of variability around loading}(\text{voxel})$$



$|Z| > 2$

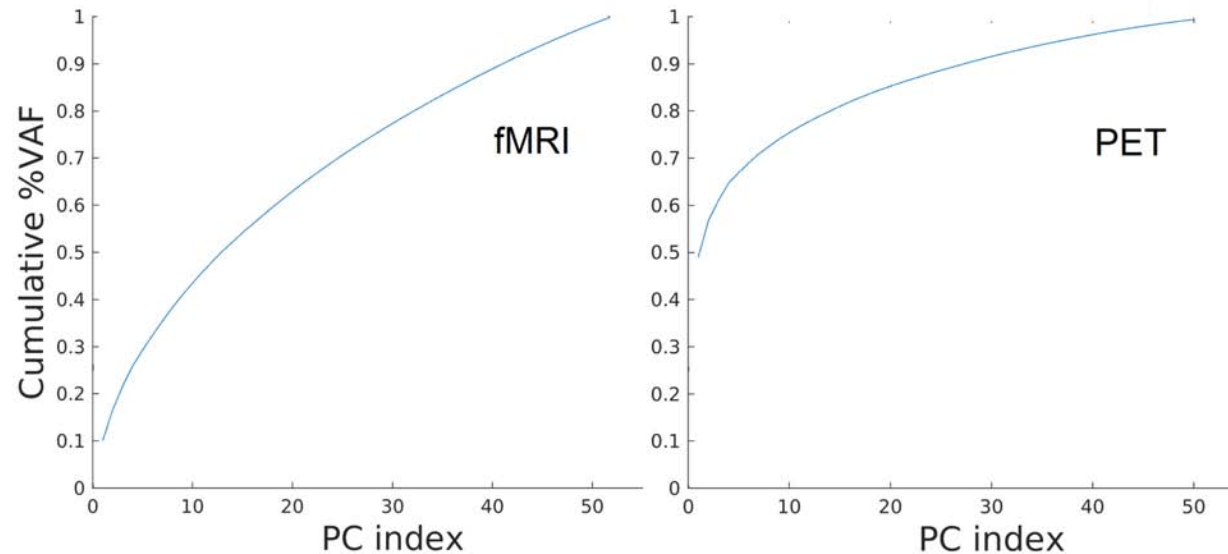
$P = 0.0083$
 $FDR = 0.05$

Conclusions

- Multivariate techniques with PCA-regression (=SSM) mark the most basic complication of traditional univariate analysis
- As a “shallow” and one-shot technique, PCA-regression offers relatively easy inferential statistics with non-parametric resampling tests, and topographic information is easily rendered
 - Attractiveness for medium sample sizes that do not yet permit deep-learning and CNNs
 - Ensemble methods like bootstrap aggregating (BAGGING) or boosting can be additionally applied for better predictive utility to better accommodate low signal-to-noise ratios
- Good reference benchmark to evaluate Deep-Learning networks in terms of predictive utility gain

Implications for molecular connectivity?

- MC potentially offers better ground-truth knowledge about regions via specific tracers and offers better variance concentration than fMRI



Courtesy of Igor Yakushev

Yakushev, Drzezga, Habeck, 2018

- For region-specific ground-truth of specific nuclei (Raphe, Nuclear Accumbens, Locus Coeruleus), seed locations could be used as “endpoints” for the derivation of patterns with the SSM (PCA-regression) technique, and further tested with mediation analysis for the relation to symptom scales/cognition

Functional notation: (pattern, pattern score) = SSM(Y, y-seed)

y-seed → pattern score → symptom scales/cognition

Thank you for your
attention

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